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Sir:

Enclosed for filing is the patent application of:

Inventor: John M. Adams

Title: UTERINE CONTRACTION DETECTION AND INITIATION SYSTEM AND METHOD

Executed:

Including:

- ☒ 1. A specification including claims consisting of 32 pages.
- ☒ 2. Formal/informal drawings consisting of 4 sheets.
- ☒ 3. Declaration and Power of Attorney.

Additionally:

4. An assignment of the invention to \_\_\_\_\_ is attached.  
X 5. A filing date in accordance with 37 CFR 1.10 is requested  
(Express mail certificate is part of this transmittal letter).  
X 6. A Small Entity Form is attached.

X 7. COMPUTATION OF FEE

	Number Filed		Number Extra		Basic Fee
Claims					\$790/\$395
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- X 8. Check No. 3009 for \$713.00 for filing fee is enclosed.  
   9. Check No.    for \$   for assignment fee is enclosed.  
   10. No fee is enclosed at this time.  
X 11. Charge any additional fees to Deposit Account No. 07-1897.  
X 12. A copy of this letter is enclosed.  
X 13. A postcard is enclosed as acknowledgment of receipt of this application.

Respectfully submitted,

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SPECIFICATION

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10  
UTERINE CONTRACTION DETECTION AND INITIATION  
SYSTEM AND METHODBACKGROUND OF THE INVENTION

15 The present invention is generally directed to a system and method for effecting uterine contractions of an animal. The present invention is more particularly directed to such a system and method for detecting and automatically stimulating contractions of the uterus of a human.

20 Prolonged pregnancy, generally classified as a gestational age exceeding 42 weeks of gestation, is associated with increased perinatal morbidity and mortality. Specifically, in addition to the increased neonatal deaths, there is an increase in the meconium aspiration, depressed infant at five minutes, and cesarean section rate. The  
25 mortality from meconium aspiration can be as high as 38% for those women managed expectantly.

Electrical energy applied to the myometrium or uterine muscle has been proposed to affect uterine contractions. One system and method to this end is disclosed in Karsdon, U.S.  
30 Patent Nos. 5,447,526 and 5,713,940 which are incorporated herein by reference. In accordance with a preferred

5 embodiment disclosed in these patents, a first or positive electrode is placed in surface contact to a woman's abdomen over the top of the uterus. Four negative electrodes are placed in spaced apart relation in surface contact to the woman's abdomen over lower portions of the uterus beginning at  
10 approximately a mid portion of the uterus. The negative electrodes and the positive electrode are then connected to a muscle controller which generates square wave pulse trains of current between the positive electrode and the negative electrodes. The muscle controller is capable of providing  
15 current pulse trains of selectable polarity. The controller is activated to inhibit uterine contractions when they are undesirably present or to initiate uterine contractions when they are undesirably absent.

In accordance with a further embodiment disclosed in the  
20 above-referenced Karsdon patents, a uterine contraction monitor is added to the system with feedback to the controller. The monitor is disposed for surface contact with the abdomen. The amount of electrical energy applied is thus responsive to the sensed contractions. The feedback may be  
25 negative or positive depending upon whether contraction initiation or inhibition is desired.

5        While the contraction monitor of Karsdon represents a significant step forward in the prenatal management of patients, there remains substantial room for improvement. The contraction monitor disclosed in the Karsdon patents is a surface monitor. Such monitors respond to physical movement.

10      As a result, physical movement which is a certainty to occur other than that of real contractions will also be sensed and create a noisy signal environment in which the contraction affecting device must respond. It would be most advantageous to have a contraction monitor which is substantially more  
15      specific in detecting uterine contractions.

         Further, surface monitors must be worn in order to function. Hence, if a patient is to be constantly monitored, the monitor must be worn at all times. This would include times of sleep and other times when such use would either be  
20      inconvenient, cumbersome, or confining.

         In addition, there is no guarantee that such a surface monitor will remain in the same place or that if removed, it will be returned to the same location on the body at a later time. This can result in signals which are variable in  
25      amplitude and other characteristics making the application of threshold criterion difficult.

5 Hence, there is a need in the art for an improved  
uterine contraction detection and stimulation system to  
initiate uterine contractions. More specifically, such a  
system must be capable of providing detection signals of good  
quality, in a low noise environment, and specific to uterine  
10 contractions. This would assure that stimulation to initiate  
uterine contractions will be provided when actually needed and  
not be provided when such stimulation is not required. The  
present invention provides such an improved uterine  
contraction detection and stimulation system.

#### SUMMARY OF THE INVENTION

15 The invention therefore provides a method of detecting  
for uterine contractions and stimulating a uterus of an animal  
having a body to initiate uterine contractions when uterine  
20 contractions are absent. The method includes the steps of  
placing first and second electrodes in contact with the body,  
the first electrode being placed in direct contact with the  
uterus, sensing electrical activity between the first and  
second electrodes, detecting for uterine contractions from the  
25 sensed electrical activity, and providing electrical current  
flow between the first and second electrodes when uterine  
contractions are undetected.

5       The invention further provides a system for detecting  
for uterine contractions and stimulating a uterus of an animal  
having a body to initiate uterine contractions when uterine  
contractions are absent. The system includes a first  
electrode, a first anchor for anchoring the first electrode to  
10 the uterus of the animal, and return current path establishing  
means for establishing a return current path within the body,  
the return current path including the first electrode. The  
system further includes a sense amplifier coupled to the first  
electrode for sensing electrical activity of the body, a  
15 detector coupled to the sense amplifier for detecting for  
contractions of the uterus from the sensed electrical activity  
and a source of electrical energy coupled to the first  
electrode and responsive to the detector failing to detect  
uterine contractions for providing electrical energy to the  
20 body along the return current path for initiating contractions  
of the uterus.

The invention still further provides a system for  
detecting for uterine contractions and stimulating a uterus of  
an animal having a body to initiate uterine contractions when  
25 uterine contractions are absent wherein the system includes  
first and second electrodes for establishing a return current  
path within the body, an anchor for releasably anchoring at



5 least one of the electrodes to the uterus of the animal, a  
detector coupled to the first and second electrodes for  
detecting for uterine contractions, and a source of electrical  
energy responsive to the detector failing to detect uterine  
contractions for applying electrical energy to the first and  
10 second electrodes for initiating contractions of the uterus.

The present invention further provides a system for  
detecting for uterine contractions and stimulating a uterus of  
an animal to initiate contractions when uterine contractions  
are absent, the system including a sensor for sensing  
15 electrical activity of the uterus, a processor for analyzing  
the electrical activity of the uterus, and an energy source  
for applying electrical energy to the uterus responsive to the  
processor when the electrical activity of the uterus fails to  
satisfy predetermined detection criteria.

20 The invention further provides a system for detecting  
for uterine contractions and stimulating a uterus of an animal  
to initiate contractions when uterine contractions are absent,  
the system including a sensor for sensing electrical activity  
of the uterus, means for storing data associated with the  
25 sensed electrical activity of the uterus, a processor for  
analyzing the stored data, and an energy source for applying  
electrical energy to the uterus to initiate contractions of

5 the uterus responsive to the processor when the analyzed data fails to satisfy predetermined detection criteria.

The invention further provides a method of detecting for uterine contractions and stimulating a uterus of an animal to initiate uterine contractions when uterine contractions are  
10 absent. The method includes the steps of sensing electrical activity of the uterus, analyzing the electrical activity of the uterus, and applying electrical energy to the uterus to initiate contractions of the uterus when the analyzed electrical activity of the uterus fails to satisfy  
15 predetermined detection criteria.

The invention still further provides a method of detecting for uterine contractions and stimulating a uterus of an animal to initiate uterine contractions, wherein the method includes the steps of sensing electrical activity of the  
20 uterus, generating data associated with the sensed electrical activity, storing the data associated with the sensed electrical activity; analyzing the stored data, and applying electrical energy to the uterus to initiate contractions of the uterus responsive to the analyzed data failing to satisfy  
25 predetermined detection criteria.

**BRIEF DESCRIPTION OF THE DRAWINGS**

The features of the present invention which are believed to be novel are set forth with particularity in the appended claims. The invention, together with further objects and advantages thereof may best be understood by making reference to the following description taken in conjunction with the accompanying drawings, in the several figures of which like reference numerals identify identical elements, and wherein:

Figure 1 is a side view, partly cut away, of a pregnant patient and a system for detecting and initiating uterine contractions having a pair of electrodes in direct contact with the patient's uterus in accordance with a preferred embodiment of the present invention;

Figure 2 is a schematic diagram of a uterine contraction detection and initiation unit embodying further features of the present invention;

Figure 3 is a partial side view to an enlarged scale and partly in cross section illustrating a first step in placing an electrode in direct contact with a uterus of a patient;

Figure 4 is a partial side view to an enlarged scale and partly in cross-section illustrating a further step in placing an electrode in direct contact with a uterus of a patient;

5 Figure 5 is a partial side view to an enlarged scale and partly in cross-section illustrating an electrode in direct contact with the uterus of a patient in accordance with a preferred embodiment of the present invention; and

Figure 6 is a side view, partly cut away of a pregnant  
10 patient and another uterine contraction detection and initiation system embodying the present invention.

#### DETAILED DESCRIPTION

Referring now to Figure 1, it schematically illustrates  
15 a pregnant patient 10 having a uterus 11 and a fetus 12 disposed within the uterus 11. The uterus 11 is enclosed by the abdominal wall 18 of the patient and includes an amniotic cavity 14 which is defined by the uterine wall 15. The uterine wall 15 is primarily comprised of the uterine muscle  
20 or myometrium 16. As is well known, the fetus 12 is disposed within amniotic fluid contained within the amniotic cavity 14.

In accordance with the present invention, a system 19 detects for and initiates contractions of the uterus 11. More specifically, the system 19 includes a detection and  
25 initiation unit 20 including a uterine contraction detector 31 and a source of electrical energy 33. The system 19 further includes first and second leads 22 and 24 having first and

5 second electrodes 26 and 28 respectively. The first and  
second electrodes are coupled directly to the uterus 11 to  
establish a current return path between the electrodes within  
the myometrium 16. As will be seen with respect to Figure 2,  
the electrodes 26 and 28 are coupled to both the detector 31  
10 and energy source 33 of unit 20.

As can be clearly seen in Figure 1, the electrodes 26  
and 28 of leads 22 and 24 respectively are in direct contact  
with the myometrium 16. The electrodes 26 and 28 are also  
preferably configured so as to be releasably anchored within  
15 the myometrium 16 as will be more particularly described  
subsequently.

In the detection of contractions of the uterus 11, the  
electrodes 26 and 28 provide an electromyographic signal (EMG)  
representing the electrical activity of the myometrium 16.  
20 Because the electrodes 26 and 28 are within the myometrium 16,  
the EMG is very specific to the electrical activity of the  
myometrium 16. When the EMG satisfies a predetermined  
criteria to be explained subsequently, uterine contractions  
are determined to be present. Conversely, when the EMG fails  
25 to satisfy a predetermined criteria, uterine contractions are  
considered to be sufficiently absent to require uterine  
stimulation for uterine contraction initiation.

5        When contractions of the uterus 11 are to be initiated,  
the electrical energy source 33 is activated by the detector  
31 to provide, for example, trains of square wave voltage  
pulses. The electrical energy is applied directly to the  
myometrium 16 along the aforementioned current return path  
10 within the myometrium by virtue of the electrodes 26 and 28  
being directly in contact with the myometrium 16. Because the  
electrodes 26 and 28 are fixedly anchored within the  
myometrium 16, they will not be dislodged by the uterine  
contractions to enable the therapy to have its complete  
15 therapeutic effect. However, because the electrodes are  
releasably anchored, they may be readily removed in a non-  
invasive manner when no longer needed.

To lend further understanding of the present invention,  
the electrical activity of the uterus can exhibit two distinct  
20 forms of activity. One form is that of a uterine contracture  
which is exhibited long before actual labor. Contractures are  
represented by bursts of electrical activity which can last on  
the order of several minutes and which are widely spaced apart  
by separations of about an hour or more. Contractures are  
25 disorganized muscle activity of the myometrium causing  
minimal, if any, physical manifestations of the myometrium.

5       The other form is that of a uterine contraction.  
Contractions are represented by relatively short bursts of  
electrical energy with the bursts being relatively closely  
spaced apart. For example, during labor, the uterine  
contraction electrical bursts of energy may have durations of  
10 thirty seconds or less with separations on the order of twenty  
minutes or less. Contractions, as compared to contractures,  
are organized muscle activity of the myometrium causing  
pronounced physical manifestations of the myometrium. It is  
the occurrence of contractions that is most identified as  
15 labor.

      The electrical energy bursts of both contractures and  
contractions are made up of electrical waves having  
separations of, for example, three hundred milliseconds to  
nine hundred milliseconds (300ms to 900ms). As will be seen  
20 subsequently, one or more characteristics of the EMG  
electrical bursts are used to identify actual contractions or  
the lack thereof in need of initiation.

      Referring now to Figure 2, it illustrates in schematic  
form, the uterine contraction detection and initiation unit 20  
25 of Figure 1. The unit 20 includes the contractions detector  
31 and energy source 33 within an enclosure 30. The unit 20  
is turned on by a switch 50 which connects a battery 51 to the

5 various components of the unit 20 when contractions are to be initiated or maintained.

Within the enclosure 30 is also a microprocessor 32 which, in a manner well known in the microprocessor art, operates on operating instructions stored in an internal  
10 memory 52 or an external memory (not shown). As a result of such operation, the microprocessor 32 implements the contractions detector 31 including burst duration stage 39, a first timer 41, an inhibit stage 45 and a second timer 47. Also, stored in memory portion 53 of memory 52, are  
15 preprogrammed contraction detection parameters or criteria.

The contraction detector 31 further utilizes a sense amplifier 35 and a threshold circuit 37. The sense amplifier 35 has a pair of inputs which are coupled to outputs 68 and 70 of the unit 20. The outputs 68 and 70 are adapted to be  
20 coupled to the first and second electrodes 26 and 28.

The electrodes 26 and 28 provide the EMG representing the electrical activity of the myometrium. The EMG is amplified by the sense amplifier 35. The amplified EMG is then provided by the sense amplifier 35 to the threshold  
25 detector 37. Whenever an electrical wave from the sense amplifier 35 exceeds a threshold magnitude set by the



5 threshold detector 37, the threshold detector will provide an output to an interrupt input 43 of the microprocessor 32.

The burst duration stage 39 time stamps each interrupt input and stores each time stamp in memory 52. It also, with timer 41, starts keeping time from each interrupt input. When  
10 the timer 45 has timed a predetermined time period of, for example, five seconds without being reset by another interrupt, the burst duration stage 39 considers the current burst to be completed. The next interrupt will then represent the beginning of the next burst of electrical activity.

15 The inhibit stage 45 precludes the energy source 33 from stimulating the uterus as long as contractions are sufficiently present. To that end, the second timer 47 starts keeping time from the beginning of each burst as determined by the duration stage 39. As long as the second timer 47 is  
20 reset by the burst duration stage 39 before it times out, the inhibit stage 45 will continue to inhibit the energy source 33. However, when a next burst fails to begin within the time out time period of the second timer 47, the inhibit stage 45 activates the energy source 33 for stimulating the uterus to  
25 initiate the next contraction. The time out period of timer 47 may be, for example, on the order of two minutes. As a result, if a next burst does not occur within two minutes of

5 its immediately preceding burst, the beginning the contraction  
detector 31 will consider the contractions to be insufficient  
and warranting uterine stimulation to initiate the next  
uterine contraction. Hence, a new contraction will be  
initiated when a uterine contraction is undetected within a  
10 predetermined time from the beginning of an immediately  
preceding uterine contraction. As can be appreciated by those  
skilled in the art, the time out period may be tailored to an  
individual patient. The above time out period is provided as  
being exemplary only.

15 The energy source 33 includes a charging circuit 34, an  
analog to digital converter 36, a storage capacitor 38, and an  
H bridge 40 comprising field effect transistors 42, 44, 46,  
and 48.

The electrical energy source 33 is activated by the  
20 inhibit stage 45 of the contractions detector 31 over a line  
49 which causes the charge circuit 34 to charge capacitor 38.

The memory 52 has storage locations 54, 56, 58, 60, and 62  
for storing preprogrammed energy delivery parameters such as  
pulse voltage, pulse polarity, burst duration, pulse interval,  
25 and pulse duration respectively. The foregoing parameters  
including the detection parameters may be stored in the memory

5 52 with a programming computer (not shown) of the type well known in the art.

The charge circuit 34 charges the storage capacitor 38 to the pulse voltage programmed at memory location 54. The output of the charge circuit 34 is monitored by the analog to digital connector 36 which provides the microprocessor with a digital representation of the output voltage of the charge circuit 34. In this manner, the microprocessor is capable of regulating or controlling the charge circuit 34 to maintain the preprogrammed pulse voltage across the capacitor 38.

15 The H bridge 40 is of the type well known in the art which is controlled by the microprocessor 32 over control lines 64 and 66 which are provided with buffers 65 and 67 respectively to accommodate required voltage swings and higher voltage applied to H bridge 40. The signals provided by the microprocessor over the control lines 64 and 66 cause the energy source 33 to provide a train of output pulses at the output terminals 68 and 70 having the pulse polarity, burst duration, pulse interval, and pulse duration as preprogrammed in memory locations 56, 58, 60 and 62 respectively of the memory 52. The output terminals 68 and 70 of the unit 20 are coupled to the leads 22 and 24 respectively as shown in Figure

5 1 to provide the electrodes 26 and 28 with the preprogrammed electrical energy.

Figures 3-5 illustrate a manner in which the electrodes 26 and 28 may be substantially non-invasively placed in direct contact with the uterus 11 through the abdomen 18 and more particularly in direct contact with the myometrium 16 in accordance with a preferred embodiment of the present invention. Referring first to Figure 3, there is illustrated, to an enlarged scale, the abdominal wall 18 and the myometrium 16. The abdominal wall includes the skin 72 and the abdominal muscle 74.

In an initial step, a removable inner needle 76 is first inserted into an introducer tube 78. The introducer tube 78 terminates in a conical surface 80 which matches the terminating conical surface 82 of the removable inner needle 76. With the conical surfaces 82 and 80 aligned as shown in Figure 3, the introducer tube 78 and removable inner needle 76 are moved in unison to pierce the skin 72 and abdominal muscle 74. Movement of the introducer tube 78 and removable inner needle 76 is terminated when the tip 84 of the needle 76 has entered the space 86 between the abdominal muscle 74 and myometrium 16 to such an extent that the conical surface 80 of the introducer tube 78 is within the space 86. Once the

5 removable inner needle 76 and introducer tube 78 are  
positioned as shown in Figure 3, the removable inner needle 76  
is withdrawn from the introducer tube 78. With the removable  
inner needle 76 thus removed from the introducer tube 78, the  
introducer tube 78 is now ready to receive the electrode 26 at  
10 the distal end of its lead 22 as illustrated in Figure 4.

The lead 22 has a cylindrical lead body with an inner  
electrical conductor 23 which contacts a conductive collar 25  
of the electrode 26. The electrode 26 has a structure 27  
secured to the collar 25 by welding, for example. The  
15 structure 27 is formed of a relatively rigid conductive wire  
29 configured as a screw-in tip. More specifically, the  
electrode structure 27 is formed in the shape of a helix so  
that when the lead 22 is introduced through the introducer  
tube 78 to an extent permitting the electrode 26 to contact  
20 the myometrium 16, rotation of the lead 22 as indicated by the  
arrow 88 causes the helical screw-in tip 29 of electrode 26 to  
screw into the myometrium 16.

When the lead 22 has been rotated a sufficient number of  
turns to fully embed the electrode tip 29 within the  
25 myometrium 16, the lead will be securely, but releasably,  
anchored within the myometrium 16. This is illustrated in  
Figure 5 where it can be seen that the helical tip 29 of the

5 electrode 26 is fully embedded within the myometrium 16. Once  
this is accomplished, the introducer tube 78 may be removed to  
thus render the lead 22 passing through the abdominal wall 18  
including the skin 72 and abdominal muscle 74 with the  
electrode 26 securely anchored to the uterus 11 and more  
10 specifically, the myometrium 16. As a result, during the  
therapy of initiating contractions of the uterus 11, the  
contractions of the uterus 11 will not dislodge the electrode  
26 from the myometrium 16. However, when therapy is no longer  
required and the electrode 26 is no longer needed, it may be  
15 readily withdrawn by just rotating the lead 22 in a direction  
opposite that shown at 88 in Figure 4 and pulling the lead  
from the patient when the tip 29 is disengaged from the  
myometrium.

Referring now to Figure 6, it illustrates a further  
20 embodiment of the present invention. Here it may be seen that  
the unit 20 is coupled directly to the myometrium through the  
lead 22 and electrode 26 as previously described while another  
lead 90 couples the unit 20 to a surface of the body of the  
patient 10 with a surface or patch electrode 92. The patch or  
25 surface electrode 92 is in surface contact with a posterior  
portion of the body of the patient 10 and more specifically,  
on the back of the patient. With such an arrangement, a

5 return current path is established between the electrodes 26  
and 90. The electrical energy from the energy source 33 of  
the unit 20 will remain concentrated in the myometrium given  
the large surface area of electrode 92 compared to electrode  
26. The fetus 12 and the body of the patient 10 will only be  
10 exposed to dispersed energy which will be well within safe  
limits for both the fetus 12 and mother 10.

While particular embodiments of the present invention  
have been shown and described, modifications may be made, and  
it is therefore intended to cover in the appended claims all  
15 such changes and modification which fall within the true  
spirit and scope of the invention.

What is claimed is:

1 1. A method of detecting for uterine contractions of a  
2 uterus of an animal having a body to initiate uterine  
3 contractions when uterine contractions are absent, the  
4 method including the steps of:

5 placing first and second electrodes in contact  
6 with the body, the first electrode being placed in  
7 direct contact with the uterus;

8 sensing electrical activity between the first  
9 and second electrodes;

10 detecting for uterine contractions from the  
11 sensed electrical activity; and

12 providing electrical current flow between the  
13 first and second electrodes when uterine contractions  
14 are undetected.

1 2. A method as defined in Claim 1 wherein the providing step  
2 is performed when a uterine contraction is undetected  
3 within a predetermined time of an immediately preceding  
4 uterine contraction.



1 3. A method as defined in Claim 1 wherein the providing step  
2 is performed when a uterine contraction is undetected  
3 within a predetermined time from the beginning of an  
4 immediately preceding uterine contraction.

1 4. A method as defined in claim 1 wherein the placing step  
2 includes anchoring the first electrode to the uterus.

1 5. A method as defined in claim 1 wherein the placing step  
2 includes passing the first electrode through skin of the  
3 animal.

1 6. A method as defined in claim 1 wherein the placing step  
2 includes releasably anchoring the first electrode to the  
3 uterus.

1 7. A method as defined in claim 6 wherein the placing step  
2 further includes anchoring the first electrode to the  
3 myometrium.

1 8. A method as defined in claim 1 wherein the placing step  
2 includes contacting the second electrode with the  
3 uterus.

1 9. A method as defined in claim 8 wherein the contacting  
2 step further includes anchoring the second electrode to  
3 the uterus.

1 10. A method as defined in claim 8 wherein the contacting  
2 step further includes passing the second electrode  
3 through skin of the body.

1 11. A method as defined in claim 8 wherein the contacting  
2 step further includes placing the second electrode in  
3 direct contact with the myometrium.

1 12. A method as defined in claim 11 wherein the contacting  
2 step further includes anchoring the second electrode to  
3 the myometrium.

1 13. A method as defined in claim 8 wherein the second  
2 electrode is a surface electrode and wherein the  
3 contacting step includes making surface contact between  
4 the second electrode and the body.

1 14. A method as defined in claim 13 wherein the contacting  
2 step further includes making surface contact between the  
3 surface electrode and a posterior portion of the body.

1 15. A system for detecting for uterine contractions and  
2 stimulating a uterus of an animal having a body to  
3 initiate uterine contractions when uterine contractions  
4 are absent, the system comprising:

5 a first electrode;

6 a first anchor for anchoring the first electrode to  
7 the uterus of the animal;

8 return current path establishing means for  
9 establishing a return current path within the body, the  
10 return current path including the first electrode;

11 a sense amplifier coupled to the first electrode  
12 for sensing electrical activity of the body;

13 a detector coupled to the sense amplifier for  
14 detecting for contractions of the uterus from the sensed  
15 electrical activity; and

16 a source of electrical energy coupled to the first  
17 electrode and responsive to the detector failing to  
18 detect uterine contractions for providing electrical

19 energy to the body along the return current path for  
20 initiating contractions of the uterus.

1 16. A system as defined in claim 15 wherein the detector  
2 includes a timer for timing the time since a last  
3 uterine contraction and wherein the source is responsive  
4 to the timer timing a predetermined time period since  
5 the last uterine contraction for providing the  
6 electrical energy for initiating contractions of the  
7 uterus.

1 17. A system as defined in claim 15 wherein the first anchor  
2 is a releasable anchor.

1 18. A system as defined in claim 17 wherein the first anchor  
2 is configured for anchoring the first electrode to the  
3 myometrium.

1 19. A system as defined in claim 18 wherein the first anchor  
2 comprises a screw-in tip.

1 20. A system as defined in claim 19 wherein the screw-in tip  
2 is a helical coil.

1 21. A system as defined in claim 19 wherein the first  
2 electrode includes structure forming the screw-in tip.

1 22. A system as defined in claim 17 wherein the return  
2 current path establishing means comprises a second  
3 electrode adapted for making electrical contact with the  
4 body.

1 23. A system as defined in claim 22 wherein the second  
2 electrode is arranged for direct contact with the uterus.

1 24. A system as defined in claim 23 further including a  
2 second anchor for anchoring the second electrode to the  
3 uterus.

1 25. A system as defined in claim 24 wherein the second anchor  
2 is arranged for anchoring the second electrode to the  
3 myometrium.

1 26. A system as defined in claim 24 wherein the second anchor  
2 is a releasable anchor.

1 27. A system as defined in claim 26 wherein the second anchor  
2 includes a screw-in tip.

1 28. A system as defined in claim 26 wherein the second  
2 electrode includes structure forming the second anchor.

1 29. A system as defined in claim 22 wherein the second  
2 electrode is a surface electrode for making surface  
3 contact with the body.

1 30. A system for detecting for uterine contractions and  
2 stimulating a uterus of an animal having a body to  
3 initiate uterine contractions when uterine contractions  
4 are absent, the system comprising:

5 first and second electrodes for establishing a  
6 return current path within the body;

7 an anchor for releasably anchoring at least one of  
8 the electrodes to the uterus of the animal;

9 a detector coupled to the first and second  
10 electrodes for detecting for uterine contractions; and

11 a source of electrical energy responsive to the  
12 detector failing to detect uterine contractions for  
13 applying electrical energy to the first and second  
14 electrodes for initiating contractions of the uterus.

1 31. A system for detecting for uterine contractions and  
2 stimulating a uterus of an animal to initiate  
3 contractions when uterine contractions are absent, the  
4 system comprising:

5 a sensor for sensing electrical activity of the  
6 uterus;

7 a processor for analyzing the electrical activity of  
8 the uterus; and

9 an energy source for applying electrical energy to  
10 the uterus responsive to the processor when the  
11 electrical activity of the uterus fails to satisfy  
12 predetermined detection criteria.

1 32. A system for detecting for uterine contractions  
2 stimulating a uterus of an animal to initiate  
3 contractions when uterine contractions are absent, the  
4 system comprising:

5 a sensor for sensing electrical activity of the  
6 uterus;

7 means for storing data associated with the sensed  
8 electrical activity of the uterus;

9 a processor for analyzing the stored data; and

10 an energy source for applying electrical energy to  
11 the uterus to initiate contractions of the uterus  
12 responsive to the processor when the analyzed data fails  
13 to satisfy predetermined detection criteria.

14 33. A method of detecting for uterine contractions and  
15 stimulating a uterus of an animal to initiate uterine  
16 contractions when uterine contractions are absent, the  
17 method including the steps of:

18 sensing electrical activity of the uterus;

19 analyzing the electrical activity of the uterus; and

20 applying electrical energy to the uterus to initiate  
21 contractions of the uterus when the analyzed electrical  
22 activity of the uterus fails to satisfy predetermined  
23 detection criteria.

1 34. A method of detecting for uterine contractions and  
2 stimulating a uterus of an animal to initiate uterine



3       contractions when uterine contractions are absent, the  
4       method including the steps of:

5               sensing electrical activity of the uterus;

6               generating data associated with the sensed  
7       electrical activity;

8               storing the data associated with the sensed  
9       electrical activity;

10              analyzing the stored data; and

11              applying electrical energy to the uterus to initiate  
12       contractions of the uterus responsive to the analyzed  
13       data failing to satisfy predetermined detection criteria.

ABSTRACT

A system and method for detecting for and initiating contractions of a uterus of a human patient employs a sensor for sensing electrical activity of the uterus of the patient.

5 Data from the sensed electrical activity is stored in memory.

A processor accesses the stored data for analysis.

Electrical energy is applied to the uterus to initiate a uterine contraction when the analyzed data fails to satisfy predetermined detection criteria.

10

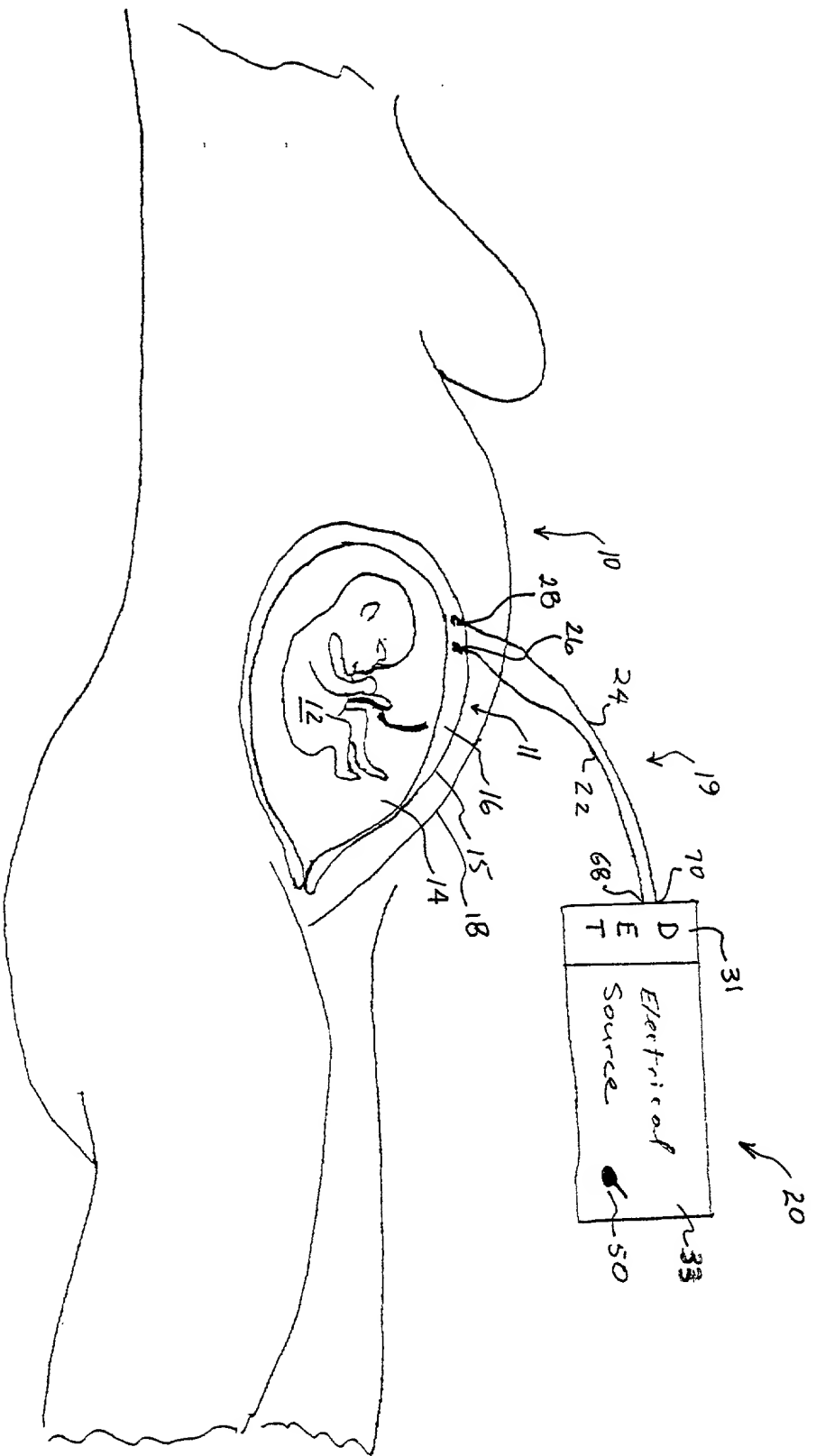


Fig. 1

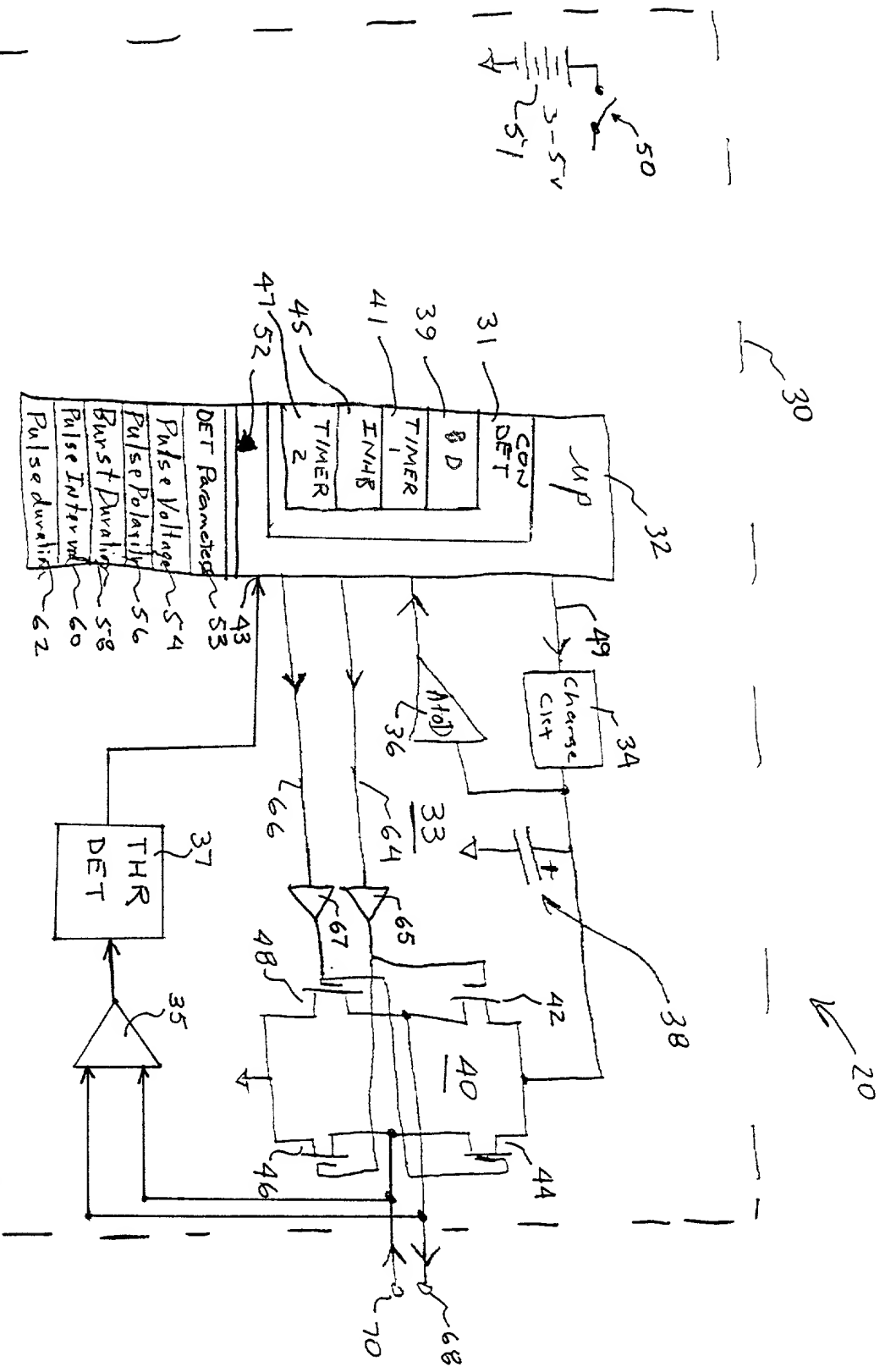
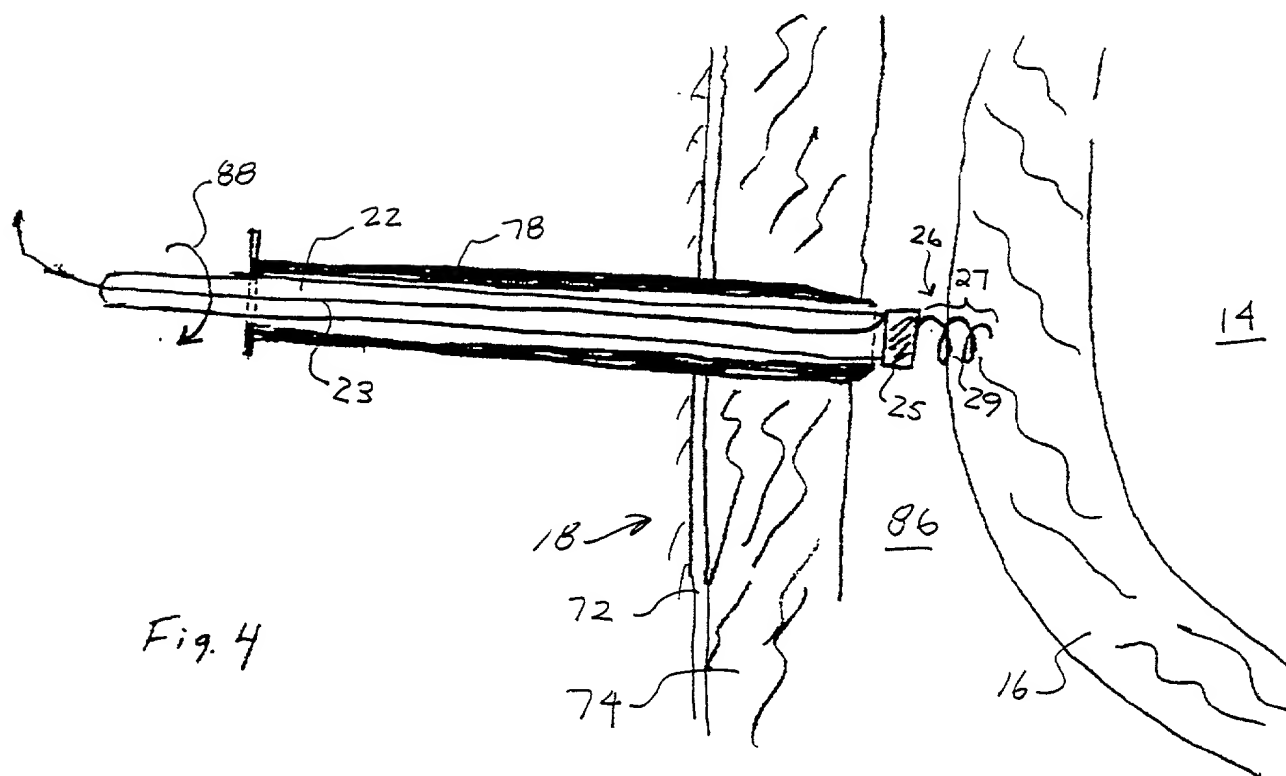
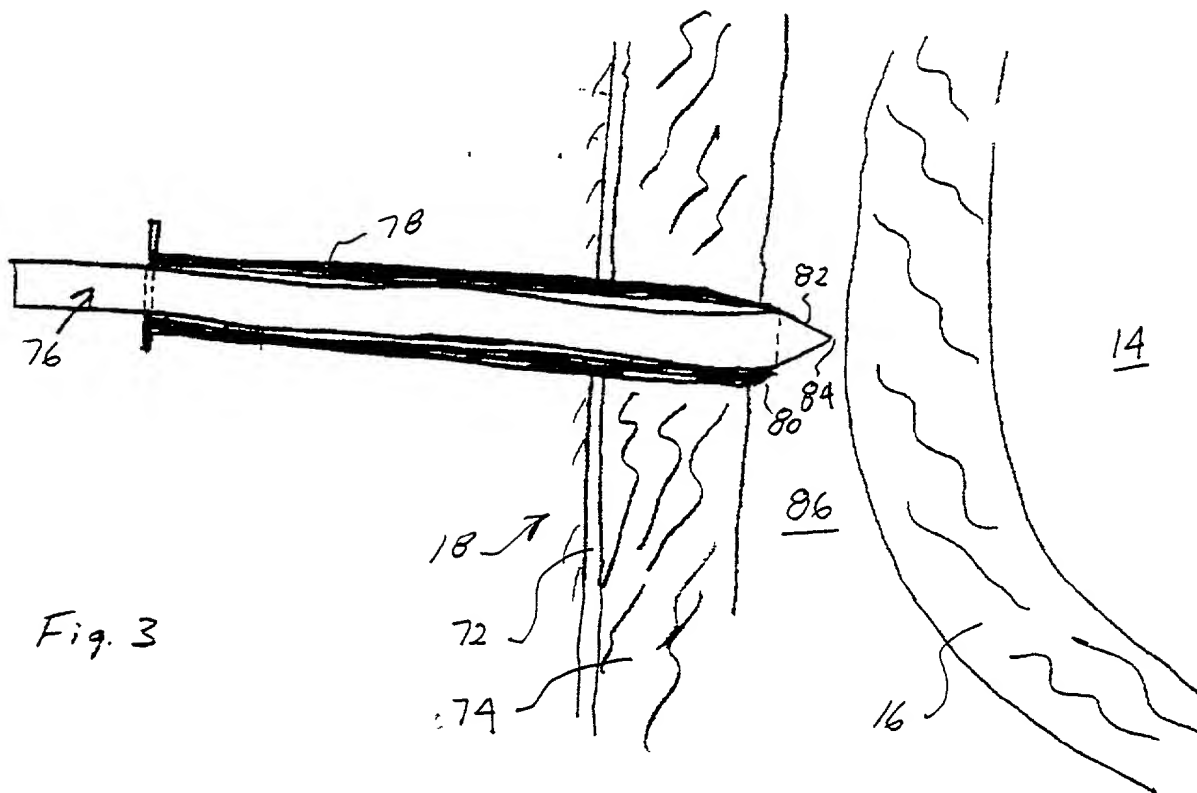
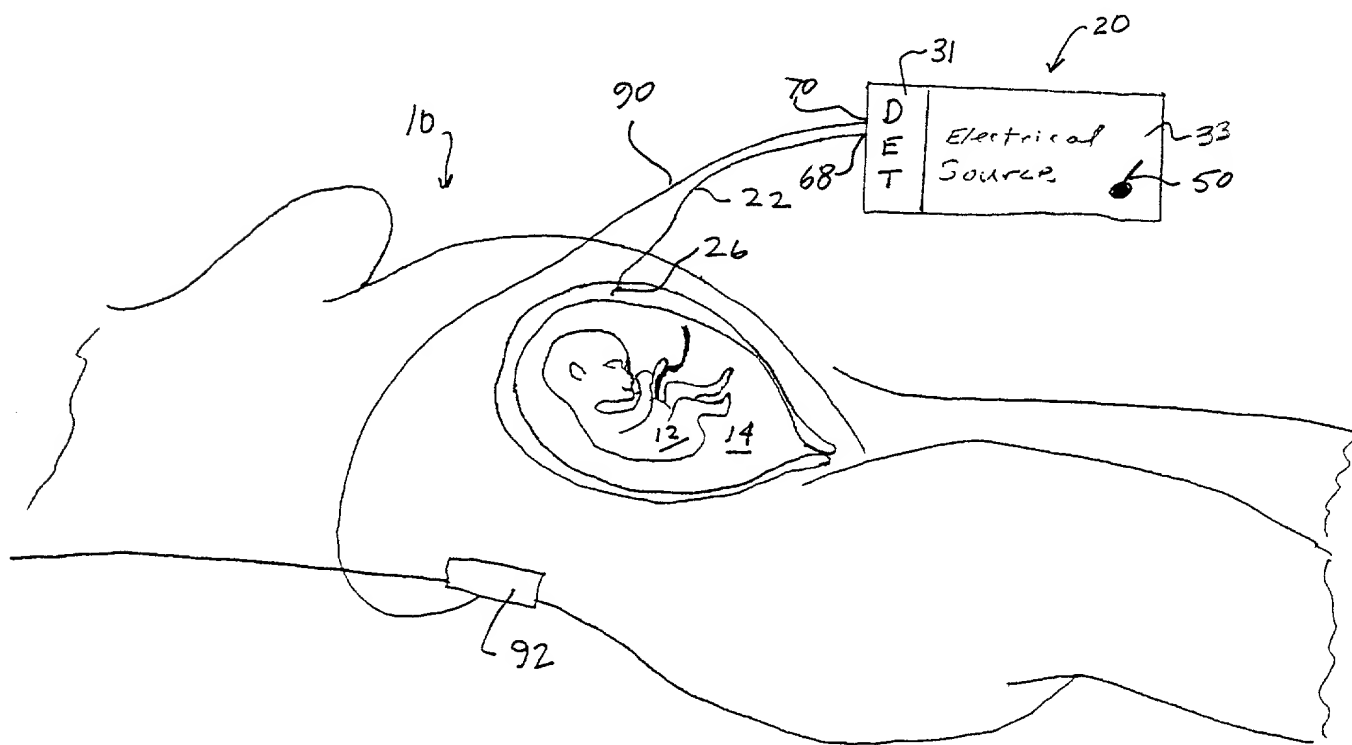
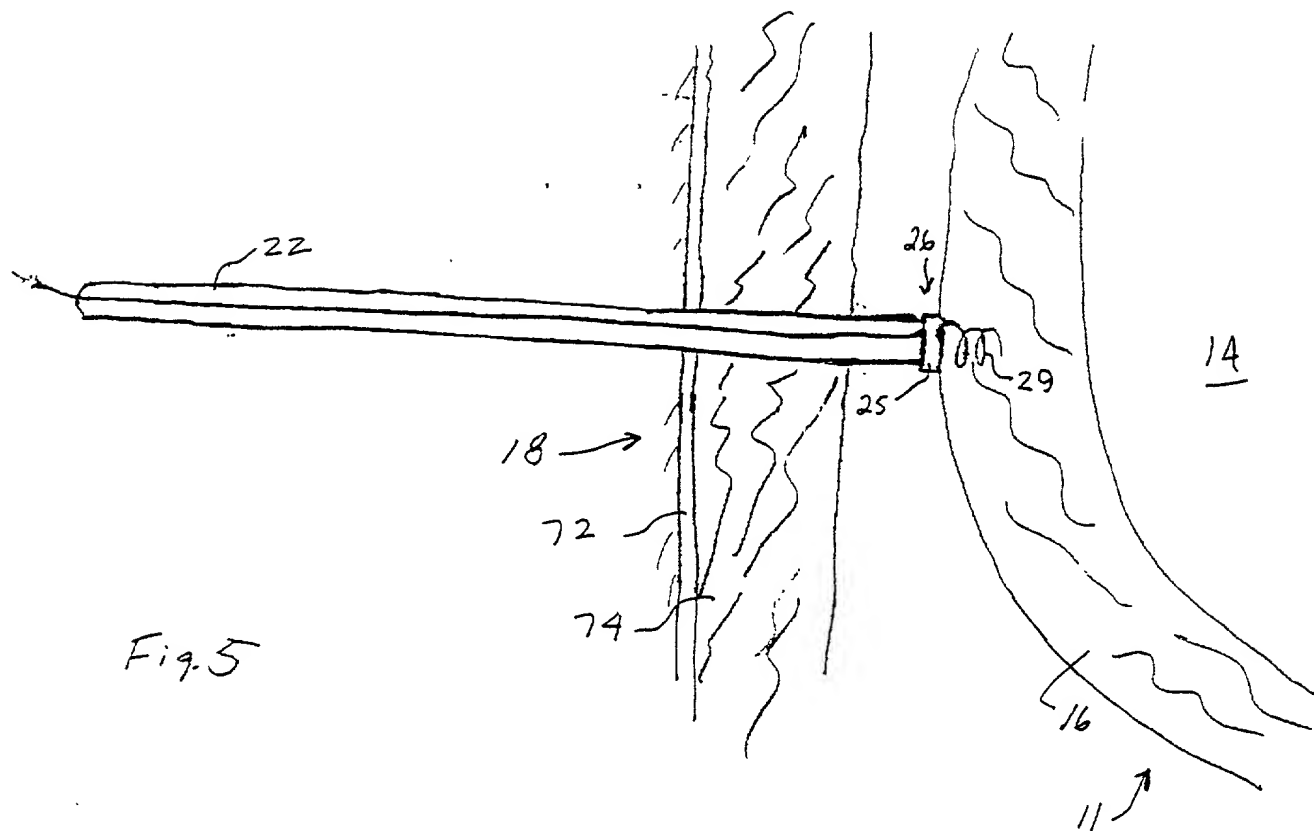


Fig. 2





05521 4305150

**DECLARATION AND POWER OF ATTORNEY  
IN PATENT APPLICATION**

Attorney Docket No.: 1696-05

As a below named inventor, I hereby declare:

My residence, post office address and citizenship are as stated below next to my name.

I believe that I am the original, first and sole inventor (if only one name is listed below) or a joint inventor (if plural inventors are listed below) of the subject matter that is claimed and for which a patent is sought on the invention entitled:

UTERINE CONTRACTION DETECTION AND INITIATION SYSTEM AND METHOD

the specification of which

- ☒ is attached hereto.
- ☐ was filed on \_\_\_\_\_ as U.S. Application Serial No. (or PCT International Application No.) \_\_\_\_\_ and was amended on \_\_\_\_\_ (if applicable).

I hereby state that I have reviewed and understand the contents of the above-identified specification, including the claims, as amended by any amendment referred to above.

I acknowledge the duty to disclose information which is material to patentability as defined in Title 37, Code of Federal Regulations, Section 1.56.

I hereby claim foreign priority benefits under Title 35, United States Code, Section 119(a)-(d) or Section 365(b), of any foreign application(s) for patent or inventor's certificate, or Section 365(a) of any PCT international application designating at least one country other than the United States listed below and have also identified below any foreign application for patent or inventor's certificate having a filing date before that of the application on which priority is claimed.

Prior Foreign Application(s):

<u>Number</u>	<u>Country</u>	<u>Date Filed</u>	<u>Priority Claimed</u>
_____	_____	_____ Day/Mo/Year	_____ Yes/No
_____	_____	_____ Day/Mo/Year	_____ Yes/No

I hereby claim the benefit under Title 35, United States Code Section 119(e) of any United States provisional application(s) listed below.

<u>Application No.</u>	<u>Filing Date</u>
_____	_____

I hereby claim the benefit under Title 35, United States Code, Section 120 of any United States application(s), or Section 365(c) of any PCT international application designating the United States listed below, and, insofar as the subject matter of each of the claims of this application is not disclosed in the prior United States or PCT international application in the manner provided by the first paragraph of Title 35, United States Code, Section 112, I acknowledge the duty to disclose information which is material to patentability as defined in Title 37, Code of Federal Regulations, Section 1.56, which became available between the filing date of the prior application and the national or PCT international filing date of this application.

<u>Application Number</u>	<u>Filing Date</u>	<u>Status: Patented Pending/Abandoned</u>
_____	_____	_____
_____	_____	_____
_____	_____	_____

I hereby appoint the attorneys associated with Customer No. 07-1897 to prosecute this application and to transact all business in the United States Patent and Trademark Office connected therewith.

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I hereby further declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code, and that such willful false statements may jeopardize the validity of the application or any patent issued thereon.

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John M. Adams

Inventor's Signature

Date

Applicant(s) or Patentee(s): John M. Adams

Serial or Patent No.: \_\_\_\_\_ Attorney Docket No: 1696-05

Filed or Issued: \_\_\_\_\_

For: UTERINE CONTRACTION DETECTION AND INHIBITION INITIATION AND METHOD

**VERIFIED STATEMENT (DECLARATION) CLAIMING SMALL ENTITY STATUS  
(37 CFR 1.9(f) and 1.27(b)) - INDEPENDENT INVENTOR**

As a below named inventor, I hereby declare that I qualify as an independent inventor as defined in 37 CFR 1.9(c) for purposes of paying reduced fees under Section 41(a) and (b) of Title 35, United States Code, to the Patent and Trademark Office with regard to the invention described in

- ☒ the specification filed herewith with the title listed above.
- ☐ the application identified above.
- ☐ the patent identified above.

I have not assigned, granted, conveyed or licensed and am under no obligation under contract or law to assign, grant, convey or license, any rights in the invention to any person who could not be classified as an independent inventor under 37 CFR 1.9(c) if that person had made the invention, or to any concern which would not qualify as a small business concern under 37 CFR 1.9(d) or a nonprofit organization under 37 CFR 1.9(e).

Each person, concern or organization to which I have assigned, granted, conveyed, or licensed or am under an obligation under contract or law to assign, grant, convey, or license any rights in the invention is listed below:

- ☒ no such person, concern, or organization.
- ☐ persons, concerns or organizations listed below.\*

\*NOTE: Separate verified statements are required from each named person, concern or organization having rights to the invention averring to their status as small entities. (37 CFR 1.27).

FULL NAME \_\_\_\_\_

ADDRESS \_\_\_\_\_

☐ INDIVIDUAL ☐ SMALL BUSINESS CONCERN ☐ NONPROFIT ORGANIZATION

I acknowledge the duty to file, in this application or patent, notification of any change in status resulting in loss of entitlement to small entity status prior to paying, or at the time of paying, the earliest of the issue fee or any maintenance fee due after the date on which status as a small entity is no longer appropriate. (37 CFR 1.28(b))

I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under Section 1001 of Title 18 of the United States Code, and that such willful false statements may jeopardize the validity of the application, any patent issuing thereon, or any patent to which this verified statement is directed.

John M. Adams \_\_\_\_\_

NAME OF INVENTOR

NAME OF INVENTOR \_\_\_\_\_

  
INVENTOR SIGNATURE

INVENTOR SIGNATURE \_\_\_\_\_

DATE \_\_\_\_\_

DATE \_\_\_\_\_